



Cardiac Magnetic Resonance Imaging Focus Generative Adversarial Network Segmentation

Maysaa Abd Ulkareem Naser ^{a,b} and Abbas H. Hassin Al-Asadi^{a*}

^aDepartment of Computer Information Systems, University of Basrah, Basrah, Iraq. Email: maysaa.naser@uobasrah.edu.iq

^b Department of Computer Science, Kufa University, Kufa, Iraq.

^aDepartment of Computer Information Systems, University of Basrah, Basrah, Iraq. Email: abbas.hassin@uobasrah.edu.iq

ARTICLE INFO

Article history:

Received: 03 /08/2023

Revised form: 23 /09/2023

Accepted : 25 /09/2023

Available online: 30 /09/2023

Keywords:

Cardiac imaging,

Generative adversarial networks(GAN),

Cardiac Segmentation,

image Segmentation by GANs

ABSTRACT

Cardiovascular function analysis is crucial for illness diagnosis, risk assessment, and therapy selection in clinical cardiology. Doctors may identify cardiac disorders such as right ventricular failure, hypertrophic cardiomyopathy, and dilated cardiomyopathy using a variety of imaging modalities that allow them to spot pathological alterations. The optimum course of therapy may be chosen more quickly thanks to accurate automation of the relevant duties. Artificial neural networks and deep learning are the foundation of generative adversarial networks (GANs), which are methods for creating synthetic pictures. The potential capacity of the GANs to solve problems has attracted interest in addition to their inherent flexibility and the adaptability of deep learning, on which they are founded. This survey aims to examine the significance of medical imaging in the study and diagnosis of cardiac disease. Demonstrate the widespread adoption of GAN Network approaches in the field of magnetic resonance imaging (MRI) medical image analysis; Explain the recent segmentation application of generative adversarial networks. GANs in cardiovascular imaging additionally Identify the hurdles to the effective application of the GAN Network to medical imaging tasks and highlight particular contributions that address or get around these problems.

<https://doi.org/10.29304/jqcm.2023.15.31291>

1. INTRODUCTION

Image data that could save lives is frequently collected in the medical imaging area [1]. These imaging techniques can produce images that show anatomical views of various human bodily organs. As a consequence of the advancement of the biomedical imaging disciplines, the data are currently given by positron emission tomography (PET), computed tomography (CT), magnetic resonance imaging(MRI), and a few more modalities including microscopy and digital pathology. However, using the available imaging data, radiologists have difficulty locating lesions with accuracy. Similar to MRI imaging, CT scanning provides extensive anatomical information and assists in accurate diagnosis.[2].

All methods of lesion tissue segmentation ask for slice-to-slice analysis on 2D format image data because these image data are given in 3D format. Slice-to-slice image data in 2D format was needed for all lesion tissue segmentation techniques. However, it will take roughly fifteen minutes per image to manually annotate medical imaging data by a radiologist or annotation specialist. The hand annotation technique is costly, time-consuming, and difficult to scale.

*Prof.Dr. Abbas H. Hassin Al-Asadi

Email addresses: abbas.hassin@uobasrah.edu.iq

Communicated by 'sub etitor'

The leading cause of death globally is cardiovascular disease [3]. Clinical AI applications have been developed to assess cardiac function and improve image quality. AI is presently revolutionizing the advancement of cardiac imaging technology and its medicinal use. [4]. Recent advances in deep learning have made it possible to use different convolution neural networks) CNN (models to solve many medical imaging problems, including image segmentation [5]. For difficult medical imaging, decision-making, deep learning models are famous for their outstanding performance [6]. These deep networks use a variety of involving transformations to abstract data at different layers, which they combine to anticipate outcomes. Deep neural networks are fully capable and necessary to create a complex link between input and predicted outcomes and possess the capacity to completely comprehend the hidden characteristics [7]. GANs, which have made remarkable strides in deep networks and have a wide variety of applications in medical imaging, have only lately attracted the interest of the research community. A subclass of deep neural networks called GANs trains two networks simultaneously. The use of GAN in medical imaging has been covered in a few studies and review papers [8]- [11]. These articles take a broad view of the study issues, which is advantageous to novice GAN scholars. However, how to use GAN for the biomedical segmentation task was not completely covered. Our study aims to comprehensively summarize the applications of GANs in segmenting biomedical images. To collect data, we used "Google Scholar" a search engine for articles with certain titles. (GANs, "Generative Adversarial Network," "GANs Segments," "GANs Medical Image Segmentation").

Most of the papers were obtained from reputable journals like "IEEE, Springer, Elsevier, and some papers from linked conferences," among others. From "arXiv" e-Print, articles with strong citations are also taken into consideration. We carefully examined each article before excluding any that did not have any bearing on biomedical imaging or GANs. We want to comprehensively summarize how AI heart imaging, including CT and MRI, has developed. First, we gave a narrative overview of the technical advancements in AI and presented the GAN approach's adaptive framework. The adaptive generative adversarial network (AGAN) is proposed to be composed of three elements: a selection generator, a discriminator, and a feature harvester. The feature extractor's function extracts pertinent features from the input data, which benefit the generative model. These features may be extracted using various methods, such as convolutional neural networks or auto encoders. The generator then employs the extracted features to generate a new set of data points. We then display the findings of a thorough literature review of current studies and discuss the clinical applications of AI and their prospects for clinical practice.

2. HEART'S ANATOMY FUNCTIONS

Two atria (top chambers) and two ventricles, totaling four compartments, make up the human heart (as shown in Fig. 1). Cardio vertebral node there is a membrane between the two heart chambers. The two sides do not immediately communicate unless there is a septal abnormality, but they do [12], [13]. The two primary types of circulatory channels that travel through the heart are the pulmonary circuit and the systemic circuit. The pulmonary circuit carries deoxygenated blood to the right atrium or half of the heart. the circulation then goes on to the lungs, where oxygen is taken in. The oxygenated blood is subsequently returned to the left ventricle via the pulmonary duct. The second pathway, commonly referred to as the systemic circuit, is used by the left ventricle (LV) to send oxygenated blood into the artery and arterial circulation. The atria and ventricles are separated by the bicuspid (mitral) and tricuspid atrioventricular (AV) valves. The cusps of the AV valves are linked to the papillary muscles, which are ventricular muscular expansions. The four phases of a healthy heart contraction are as follows. In early diastole, the heart is initially at rest. The atrium closes during the atrial systole phase, forcing blood into the ventricles. Third, the ventricles constrict until they are fully emptied while maintaining a consistent volume. In the last phase, they stop tightening, unwind, and restart the cycle. [14].

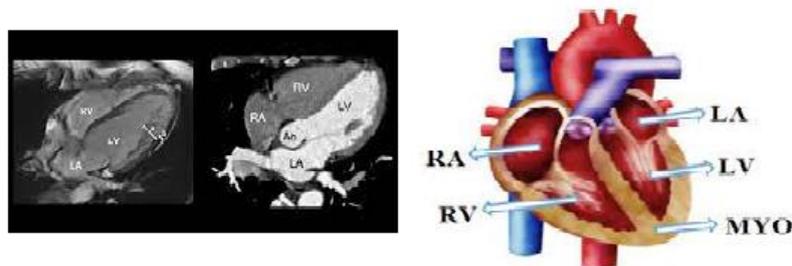


Fig.1. Human heart anatomy (atria and ventricles).

3. CARDIAC MAGNETIC RESONANCE IMAGING

Measurements of ventricular capacity and mass are needed to evaluate cardiovascular illnesses. The go-to imaging method for quantitative research is often cardiac magnetic resonance (CMR) [15], [16]. Medical image analysis commonly uses motion SSFP, first-pass stress perfusion images, and late gadolinium enhancement (LEG) images in CMR image modules. The initial criteria for rating image quality were established, among the factors limiting the quality of CMR images are well-known frequent picture artifacts. Applying certain criteria to each sort of image series, such as the CMR image modules listed above, can yield a numerical score that represents the overall picture quality of the CMR research and its three modules.

4. CMR IMAGE QUALITY ASSESSMENT CHALLENGES

CMR imaging offers a non-invasive approach to cardiac anatomy and function for population imaging research [17]. To assess cardiovascular diseases, it is essential to quantify ventricular anatomy and function using patient cohorts from lengthy clinical large-scale imaging studies or trials. Tools for image analysis and automatic image quality evaluation are needed for this quantification. The development of reliable and accurate image analysis tools for quantitative assessment is needed due to the technological constraints of imaging systems. For such systems to be used in clinical diagnosis, precise predictive performance, accessibility, and interpretability are also requirements.

4.1. CMR imaging anomalies with a defined boundary

There are not many clinical or non-clinical guidelines that specify what constitutes an excellent medical picture and CMR investigation [18].

4.2. Methods for limited quality evaluation in video editing

For automatically determining the quality of photos, a substantial corpus is available. Several techniques for video processing can identify visual distortions in frequently occurring multimedia interactions [19] [20].

4.3. Recognizing connections in cross-modality imaging data

When evaluating image clarity in medical image analysis, it may be advantageous or even vital to infer a picture from one modality from an image from another. The difficulty of CMR slice posture prediction arises from the disparity of data sources.

5. CARDIOVASCULAR IMAGING METHOD

The application of AI in cardiac imaging has been explained using two different strategies. To anticipate diagnostic or prognostic outcomes utilizing multiple clinical and pre-computed image attributes, large datasets have been employed to train traditional ML algorithms. Images from the actual world have been diagnosed using deep learning (DL) techniques, a more sophisticated kind of AI. DL does not, in contrast to conventional intelligence techniques. Direct image interrogation is utilized for tasks like image segmentation or result projection instead of "feature engineering," which computes and extracts "custom-tailored" imaging variables. Examples of huge, complex datasets with a range of properties that are good candidates for DL are imaging and genomics datasets. The underlying concept of:

Classical AI is that by automatically and repeatedly changing the appropriate weighting. It is possible to combine several weak basic classifiers to create a single potent classifier. Each iteration results in a new weighting distribution and basic classifier predictions. These projections are then used to create the weighted majority voting-based ML hazard rating, which represents a continuing assessment of the potential threat and runs from 0 to 1. Automatic feature selection using Logit Boost model construction information gain ranking and 10-fold cross-validation were all done using machine learning an ML score for risk integrating clinical and CTA evaluation is superior to accepted risk indices and visual CTA evaluation. The area under the curve (AUC) for the prediction of mortality (ML AUC = 0.79) revealed much more information. [21]. The best data on all-cause mortality after age was found in the percentage of segments with cemented and no calcified plaque. [22]. In the MESA ("Multi-Ethnic Study of Atherosclerosis") study, artificial intelligence (AI) outperformed coronary calcium scoring (CCS) in forecasting negative cardiovascular outcomes in more than 6,800 asymptomatic participants. [23]. A coronary composite risk number ('ML AUC = 0.83 vs. CTA Stenosis = 0.66') has been demonstrated to considerably increase the ability of ^{13}N -ammonia positron

emission tomography to detect decreased myocardial flow reserve. [24]. The prediction of ischemia specific to individual lesions has also been done using AI. Using CT angiography, the NXT research, in which 254 patients had CTA before invasive coronary angiography with fractional flow reserve, it was discovered that an assessment of plaque features improved the differentiation of lesion-specific ischemia. (FFR) [25]. A related research looked at the viability of using AI to forecast lesion-specific ischemia while incorporating clinical information and precise assessments of stenosis and plaque from CTA, this combination produced a higher AUC for predicting ischemia when compared to the pre-test likelihood of coronary artery disease or quantitative CTA metrics. ("ML AUC = 0.84 vs. best clinical score = 0.63, CTA stenosis = 0.76, low-density no calcified plaque volume = 0.77; p 0.006") Software applications can incorporate these machine learning risk scores to improve patient risk assessment. The clarity of CTA images has also been evaluated using the random forest method, and the findings are similar to those of expert visual assessment [26]. The groundbreaking study by Krizhevsky and Hinton [27]. 1.3 million images containing more than 1,000 distinct objects were automatically classified using Deep learning. The result of DL could be an interpretation, forecasting, diagnosis, or (more frequently) a changed photograph, such as the dataset's anatomical labels or a higher-quality image.

Deep learning (DL) has been suggested for several medicinal diagnostic applications. DL's outstanding accomplishment in computer vision, together with advancement over the last two years. Two factors that have contributed to this growth are recent advancements in reasonably priced graphics processing units ("created for the computer gaming business") and a range of DL toolkits that are open-source and accessible to all academics. The performance of fully automated segmentation, identification, and categorization of organs or lesions utilizing DL algorithms has been much enhanced compared to traditional methods. Pathology image analysis has been the most widespread application, however, numerous techniques for analyzing cardiac images have lately been put forth (as shown in Fig. 2). Cardiologists have employed DL to determine the coronary centerline. LV image segmentation, CCS from CMR, CT, and sonar images, and [28], [29]. The availability of freely available training image datasets made the research possible. More for CMR, where a sizable open archive has already been created. The 2016 Kaggle CMR competition's winning teams calculated the LV volumes using a DL technique Researchers employed complete automation to measure LV volumes. In one documented instance of this research, 1,340 subjects underwent training and validation. [30].

An automatic DL algorithm's training and evaluation for identifying a severe angiographic disease from SPECT MPI by Betancur et al. [31] utilizing the most current registry (" 1,638 SPECT MPIs from the REFINE SPECT") Use of SPECT cameras is advised for patients with possible coronary artery dysfunction. [32]. To control memory and processing effectiveness, instead of using complete 3D image datasets, they used displays for automatically produced 2D polar maps as the convolutional neural network's initial input. Each vascular territory's obstructive condition was trained into the DL network. This technique (which distinguished between training and test data using cross-validation) beat the industry standard for quantifying these images. Despite not having the specialized graphics card used for system instruction, the pre-trained model assessed a brand-new patient in less than one second.

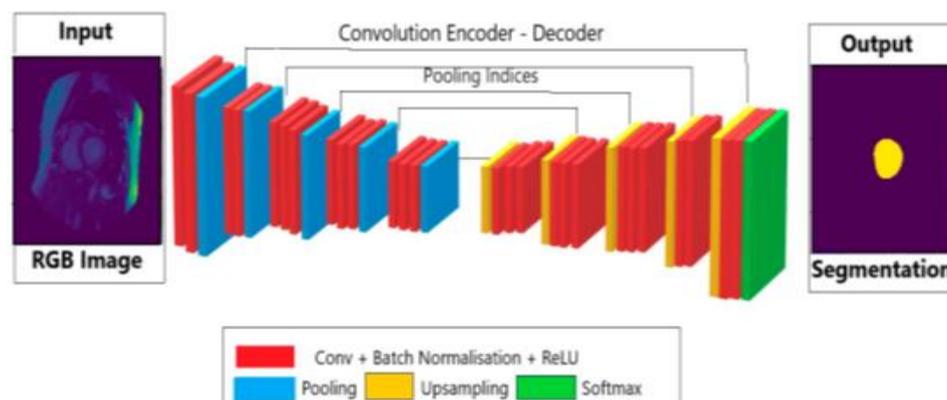


Fig. 2. Example of context-enabled Encoder-Decoder segmentation [33].

6. CARDIAC MR IMAGE SEGMENTATION

Heart image segmentation is crucial for obtaining accurate diagnosis of heart disorders and for giving information that will be helpful during clinical therapy and surgery. MRI is the modality most frequently used to produce cardiac pictures (as shown in Fig. 3). Segmentation is a helpful technique for examining the quantitative function and

perfusion of cardiac MR images. By tracking left ventricular volume (LVV) over the cardiac cycle, as well as associated indices including ejection percent, wall thickness during the cardiac cycle, and left ventricular myocardium mass (LVMM), it provides an accurate and quick diagnostic of the heart.

The analysis and interpretation of CMR images are often time-consuming. Cardiac features like the left ventricular wall can significantly decrease the automated segmentation of the time required for image processing. To automate this process, several techniques have been suggested. These techniques can be classified as deep learning or non-deep learning techniques. An overview of the steps required to divide heart pictures into the following categories: Multi-Chamber, Left Ventricle, Right Ventricle, Aortic Valve, Left Atrium, and Right Atrium.

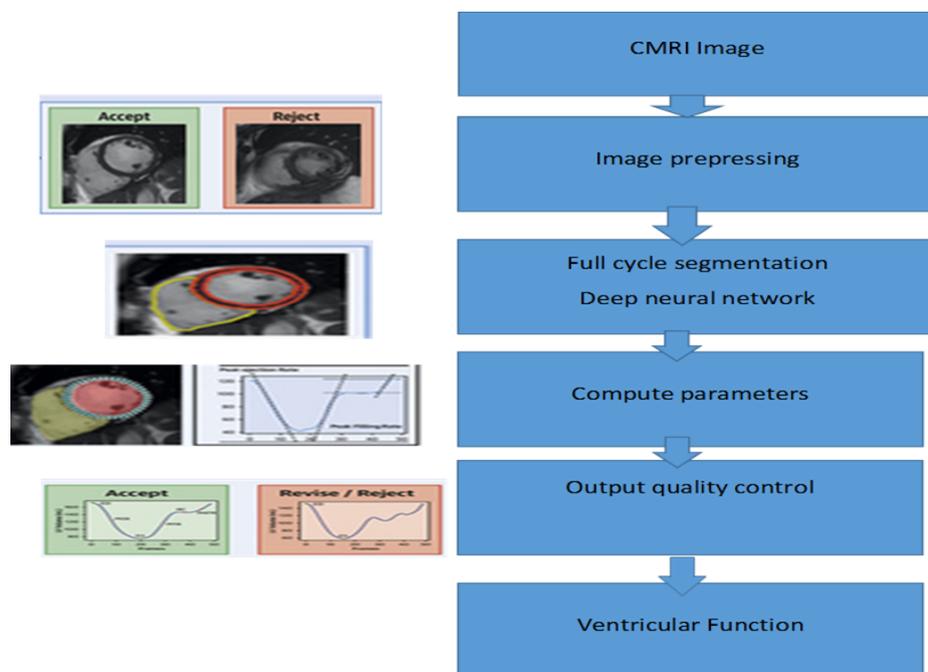


Fig. 3. An overview of the tasks involved in segmenting heart images.

7. GAN APPLICATION IN CARDIAC IMAGING

The applications of the GAN model in different biomedical imaging methods are discussed in this section (as shown in Table 1). Heart diseases, clinical monitoring, and therapy planning all stand to benefit greatly from cardiovascular segmentation in medical imaging. Because it contains information on premedication and surgical procedures, the information given by cardiac magnetic resonance imaging (CMRI) helps, evaluate all possible therapies. However, echocardiogram encounters some challenges, including poor spatial precision, deformable appearance, and a lack of readily available annotation images.

8. GAN-based derivative models

Since (Goodfellow et al). [34] proposed a GAN in 2014 There have been several GAN-based derivative models presented. These models combine cutting-edge theoretical advancement, model construction, and application principles. Semi-GAN was suggested by Odena et al. [35], who improved the training of the discriminator D with knowledge from real data annotation. [36] Another suggestion was to employ the conditional GAN ("CGAN") by incorporating y , which may be labels or other supplementary data, into the model. Traditional GANs create a generative model to connect the distribution of the data from the hidden layer with that of the real data and other data. (As shown in Fig. 4).

In this particular version, the input to generator G is split into z and c , where z is identical to the input to the GAN and c denotes the implicit connection between a given semantic and a set of hidden structural variables. $pG(x) = pG(x | c)$ in a GAN. However, there is a significant connection between c and the outcome of G . The output of the generator is

shown by the equation $G(z, c)$. Given that a GAN cannot construct a discrete space distribution and can only produce a continuous real number distribution, [37]"Browne et al." Our proposed SeqGAN enhances GANs with the RL-based generator to handle the issue of sequence creation, where the discriminator sends a reward signal after each sequence. Monte Carlo technique. Table 2 lists the GAN model's advantages and disadvantages.

Table 1. The articles for cardiac segmentation using GAN models are summarized.

Reference	Type GAN	Method description
[53]	Automap-GAN	Our approach is based on the newly created Automap reconstruction technique, which uses deep learning to directly recreate high quality MR images from k-space.
[54]	Network CCGAN	Suggest a technique for bi-ventricle segmentation that is automatic and concurrent. First, we select the area of interest (ROI) from the initial cardiac image at various sizes. The captured ROI is then fed into the conditional convolution generative adversarial network (CCGAN), which creates a segmentation overlay.
[55]	Unet-GAN	Proposed a comprehensive architecture to solve this issue, consisting of (1) a vendor adaption GAN for unpaired GANs and (2) object segmentation GANs. The Unet-GAN concept that is being suggested calls for GAN to obtain feature data from Unet at the feature level. However, we choose cardiac cine MRI as the example, with three significant manufacturers functioning as three zones (Philips, Siemens, and GE). The method may be used to extensively segment medical pictures.
[56]	SDNet (U-Net and GAN)	A cycle-consistency-based approach to latent space decomposition is suggested. Consider the implementation of cardiac MR segmentation, where data about the myocardium is separated from imaging-related characteristics and auxiliary substructures.
[57]	conditional GANs	Dividing the myocardial of individuals with congenital heart disease using a chain of conditional GANs for semantic segmentation
[58]	CGAN(VoxelAtlasGAN.)	Utilized in 3-D echocardiography to divide the LV. This network combines map into a framework augmentation from start to finish and is built using voxel-to-voxel-based cGAN. The findings highlight how crucial the suggested paradigm is for clinical applications.
[59]	VAE-GAN	For the implementation of cine-MR image cardiac segmentation, we suggest a Variation Auto encoder (VAE) - Generative Adversarial Net-works (GAN) model can generate highly realistic MRI along with its pixel exact ground truth.
[60]	CGAN U-Net	To capture these interactions, suggest a machine learning technique that uses a conditional Generative Adversarial Network (cGAN) to predict cardiac deformation from individual cardiac magnetic resonance (CMR) frames and learns a deterministic mapping between end-diastolic (ED) and end-systolic (ES) CMR short-axis frames.
[61]	AAE	For both discrete and continuous hidden variables in probabilistic autoencoders, the GAN framework has been presented as a variational inference method. On the real-valued MNIST and Toronto Face datasets, the adversarial autoencoder (AAE) approach we use creates rival test likelihoods.
[62]	GAN-based (U2S network)	A few-shot GAN Transfer Learning for Interactive Echocardiography Translation was suggested in the article. Both the U2S Parent Network and the S2U Parent Network have been previously developed and retrained.
[63]	GANs (PSCGAN)	Progressive sequence causal GANs (PSCGAN) are suggested in this paper. This is the first comprehensive CA-free IHD approach that can simultaneously create an LGE-equivalent image from cine MR images and segment tissues crucial for diagnosis (such as scars, healthy myocardium, blood pools, and other pixels).
[64]	Unet-GAN	In the suggested Unet-GAN design, GAN picks up segmentation-specific feature information from Unet at the feature level. The technique can be applied to the segmentation of medical pictures generally, However, we chose cardiac cine MRI as the illustration, with three important manufacturers (Philips, Siemens, and GE) acting as three areas
[65]	progressive sequential causal GANs)	(1) Generating a crude tissue overlay in advance with GAN. (2) LGE analogous picture synthesis GAN condition. (3) GAN with precise segmentation.
[66]	(MuTGAN)	Complementarity between segmentation and measurement (A1): joint feature learning network for multitask learning (A2): spatiotemporal feature extraction network by 3D sequential convolution; kinematic abnormalities and LV morphology (A1): combined feature learning network for multitask learning; The (B) discriminator (B1) is the task-relatedness network, which uses task-relatedness patterns as an innate structure between occupations.
[67]	(R2Unet-GAN)	The R2U-Net serves as the generating network and the FCN operates as the discriminative network in the network design, which is based on a conventional architecture known as a conditional generative adversarial network (cGAN).
[68]	DT-GAN	To decrease the number of pictures needed for training while keeping high segmentation accuracy, we therefore present a semi-supervised semantic segmentation method.
[69]	(DAN) model	A novel deep adversarial network (DAN) model is proposed to achieve reliably effective segmentation results on both annotated and unannotated pictures in the field of biomedical imaging.

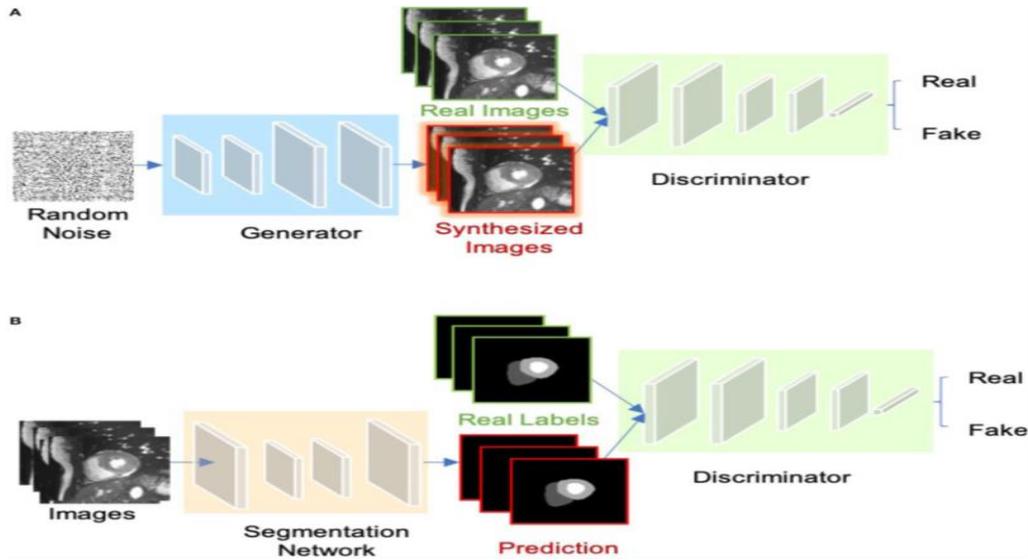


Fig. 4. (A) GAN for image synthesis overview. (B) A description of antagonistic training for segmenting images. [38]

Table 2. Some previous studies of the GANs network in terms of the advantages and disadvantages

Model	Advantage	Disadvantage
DCGAN[39]	Model stability and picture processing suitability	Model bursts, gradient vanishes, and it's uncontrollable
CGAN[40]	Controllable training	Gradient vanishes, model erupts
WGAN[41]	can stop the eruption of gradient disappearance; more stable	Selecting a weight-cutting range can be challenging.
INFOGAN [42],[43]	comprehensible example features	Gradient vanishes, model erupts
BEGAN[44]	The model is simpler to train and the generated sample diversity is superior	Model bursts, the gradient vanishes, and it's uncontrollable
CycleGAN[45]	Training rounds don't need to be paired	substantial use of processing resources
SRGAN[46]	Low-resolution photos are scaled up by 4x to create high-resolution images.	There is some disturbance and not enough realistic texture information
ACGAN[47]	For each division, accuracy can be evaluated	Overlooks the damage that class labels do when a label is missing from a particular training picture.
LAPGAN[48]	training independently for each pyramid stage	No convergence and mode collapse
SAGAN[49]	Recent studies have shown that generator conditioning affects GAN performance, and improves training dynamics.	Focus is not Expanded
GRAN[50]	Sequential generation of images	Samples break down after extensive training
AAE [51]	Balanced approximation is superior to vibrational autoencoders and can be expanded to semi-supervised learning	Examples produced are fuzzed and smoothed
Pix2Pix[52]	The generation of realistic pictures and parameter reduction	Images must be paired one to one.

9. CHALLENGES

Despite their ability to generate data, GANs have associated disadvantages that may prohibit them from accepting data synthesis software. The following list includes some of these restrictions:

1. Dynamics Instruction. The training process with GANs is unstable and unpredictable due to their adversarial structure. Mode collapse, where GAN's generator only learns to create a subset of a reference dataset, limits the trained model's usefulness.
2. Another problem is the long training times for advanced GAN models; even modern graphics processing units take weeks of training.
3. Model Evaluation. Since it is challenging to objectively assess Uncertainty exists regarding model convergence and the quality of the generated pictures, and dynamics instruction is made more difficult.

4. Medical Clinicians must exercise caution when implementing new tools because their choices influence their patients' health. Because they fall under the category of "black-box" probabilistic models, the behaviour of the neural networks that constitute the core elements of GANs is not completely understood [70].
5. Additionally, the intricate features of an organ or pathology may not be fully captured in GAN images. These issues need to be fixed for GANs to be accepted as reliable therapeutic tools.
6. Data Ethics and Rules. Because it is so closely related to a person's health details, medical data is extremely sensitive. In light of this, it is still unclear whether data laws and regulations protect Synthetic data generated by GANs trained on actual patient data.
7. GANs have the potential to amplify the biases inherent in the original datasets, which poses ethical questions about the use of GAN-generated data as a trustworthy source of information

10. DATA AVAILABILITY

Dataset /References	Link
York:10[71]	http://www.cse.yorku.ca/~mridataset
Sunnybrook [72]	http://www.cardiacatlas.org/studies/sunnybrook-cardiac-data/
LVSC:[73]	http://www.cardiacatlas.org/challenges/lv-segmentation-challenge/
RVSC [74]	http://www.litislab.fr/?projet=lvsc
cDEMIRIS:[75]	https://www.doc.ic.ac.uk/~rkarim/la_lv_framework/fibrosis
LVIC:[76]	https://www.doc.ic.ac.uk/~rkarim/la_lv_framework/lv_infarct
LASC*13:[77]	http://www.cardiacatlas.org/challenges/left-atrium-segmentation-challenge/
HVSMR:[78]	http://segchd.csail.mit.edu/
ACDC:[79]	https://acdc.creatis.insa-lyon.fr/
LASC*18:[80]	http://atriaseg2018.cardiacatlas.org/data/
MM-WHS:[81]	http://www.sdpeople.fudan.edu.cn/zhuangxiahai/0/mmwhs17/
CAT08:[82]	http://coronary.bigr.nl/centerlines/
CLS12:[83]	http://coronary.bigr.nl/stenoses
CETUS:[84]	https://www.creatis.insa-lyon.fr/Challenge/CETUS
CAMUS:[85]	https://www.creatis.insa-lyon.fr/Challenge/camus

11. CONCLUSION

This article summarized a thorough analysis of cardiac magnetic resonance imaging and GAN including their fundamental concepts, GAN variants, cardiac MR image segmentation by GAN, and their visual perception-related computational uses. A comparison between biological and computer vision is made to better comprehend the development of neural networks and the background of computer vision. This poll offers a thorough comparison of recent and previous surveys. This study in-depth examines GAN's uses in cardiac MR image segmentation. It has been demonstrated that GAN can address the issue of insufficient data and enhance picture generation quality. The experimental results are discussed to examine the capabilities of GAN model variations. The benefits, disadvantages, and network designs of several GAN models are explained. Cardiac MR Image Segmentation and GAN applications are also addressed, both of which have made significant progress in many computer vision applications. The possibilities and difficulties in all the emerging areas are covered in depth in this article. One of the potential directions for future study is to modify GAN in this manner.

REFERENCES

- [1] T. McInerney, D. Terzopoulos, "Deformable models in medical image analysis: a survey", *Med Image Anal*, Volume1, Pages 91-108(1996), [https://doi.org/10.1016/S1361-8415\(96\)80007-7](https://doi.org/10.1016/S1361-8415(96)80007-7).
- [2] S. Hussain, I. Mubeen, N. Ullah, S. Shahab, et al., "Modern Diagnostic Imaging Technique Applications and Risk Factors in the Medical Field: A Review", *BioMed Research International*, vol. 2022, 19 pages (2022). <https://doi.org/10.1155/2022/5164970>
- [3] A. Iqbal, M. Sharif, "MDA-Net: Multiscale dual attention based network for breast lesion segmentation using ultrasound images," *Journal of King Saud University –Computer and Information Sciences*, Volume 34, Issue 9, Pages 7283-7299(2022). <https://doi.org/10.1016/j.jksuci.2021.10.002>
- [4] G. Litjens, T. Kooi, B. Bejnordi, A. Arindra, F. Ciompi et al., "A survey on deep learning in medical image analysis, *Med Image Anal*," 42:60-88(2017), doi: 10.1016/j.media.07.005.
- [5] D. R. Sarvamangala and R. V. Kulkarni, "Convolutional neural networks in medical image understanding: a survey," *Evolutionary Intelligence* volume 15, pages 1–22 (2022).
- [6] A. Singhal, M. Phogat, D. Kumar, A. Kumar, M. Dahiya, V.K. Hrivastava, "Materials Today: Proceedings, "Study of deep learning techniques for medical image analysis, Volume 56, Pages 209-214(2022).
- [7] I. Arel, D. C. Rose and T. P. Karnowski, "Deep Machine Learning - A New Frontier in Artificial Intelligence Research [Research Frontier]," in *IEEE Computational Intelligence Magazine*, vol. 5, no.4, pp.13-18, Nov.2010, doi:10.1109/MCI.2010.938364.

- [8] X . Yi, E . Walia, P . Babyn,” Generative adversarial network in medical imaging: a review,” *Med Image Anal*, Volume 58,(2019) <https://doi.org/10.1016/j.media.2019.101552>
- [9] S. Kazemina, C. Baur, A. Kuijper, et al, “GANs for medical image analysis,” *Artif Intel Med*, Volume 109, 101938, (2020). <https://doi.org/10.1016/j.artmed.2020.101938>
- [10] V . Sorin, Y . Barash, E . Konen, E . Klang,” Creating artificial images for radiology applications using generative adversarial networks (GANs)—a systematic review,” *Acad Radiol*, Volume 27, ISSUE 8, P1175-1185 (2020) <https://doi.org/10.1016/j.acra.2019.12.024>.
- [11] P.Kumar MR, P. Jayagopal,” Generative adversarial networks: a survey on applications and challenges,” *International*,10,pages1–24 (2021)<https://doi.org/10.1007/s13735-020-00196-w>
- [12] S. Standring, *Gray's Anatomy E-book: The Anatomical Basis of Clinical Practice*, Elsevier Health Sciences, (2015).
- [13] L. H. Opie, *Heart Physiology: From Cell to Circulation*, 4th Edition Lippincott Williams &Wilkins, (2004).
- [14] M. P. Nash and P. J. Hunter, “Computational Mechanics of the Heart,” *Journal of Elasticity and the Physical Science of Solids* volume 61, pages113–141 (2000)
- [15] S. Conolly, A. Macovski, J. Pauly, J. Schenck, K. K. Kwong, D. A. Chesler, X. P. Hu, W. Chen, M. Patel, and K. Ugurbil, “Magnetic Resonance Imaging,” In *Medical Devices and Systems*, pages 243–282(2006). CRC Press.
- [16] R. W. Brown, E. M. Haacke, Y. C. N. Cheng, M. R. Thompson, and R. Venkatesan, *Magnetic Resonance Imaging: Physical Principles and Sequence Design*. John Wiley & Sons, (2014).
- [17] E. Castillo, J. AC. Lima, and D. A. Bluemke,” Regional Myocardial Function: Advances in MR Imaging and Analysis,” *Radiographics*, 23(suppl 1): S127–S140(2003).
- [18] A. Graaf, P. Bhagirath, S. Ghoerbien, and M. G“otte, *Cardiac Magnetic Resonance Imaging: Artefacts for Clinicians*, *Netherlands Heart Journal*,22(12):542–549(2014).
- [19] M. A. Saad, A. C. Bovik, and C. Charrier, “Blind Image Quality Assessment: ANatural Scene Statistics Approach in the DCT Domain,” *IEEE Transactions on Image Processing*, 21(8):3339–3352(2012).
- [20] M. Motwani, D. Dey, D. Berman, et al., “Machine learning for prediction of all-cause mortality in patients with suspected coronary artery disease: a 5-year multicenter prospective registry analysis,” *Eur Heart J*;38:500–7, [PubMed: 27252451], (2017).
- [21] R. Nakanishi, D. Dey, F. Commandeur, et al.,” Machine learning in predicting coronary heart disease and cardiovascular disease events: results from the Multi-Ethnic Study of Atherosclerosis (MESA) (abstract),” *J Am Coll Cardiol*,71: A1483, (2018).
- [22] D.Dey, M. Zamudio, A. Schuhbaeck, et al.,” Relationship between quantitative adverse plaque features from coronary computed tomography angiography and downstream impaired myocardial flow reserve by 13N-ammonia positron emission tomography: a pilot study,” *Circ Cardiovasc Imaging*, 8:3255–65(2015).
- [23] S. Gaur, K. ovrehus, D. Dey, et al.,” Coronary plaque quantification and fractional flow reserve by coronary computed tomography angiography identify ischemia-causing lesions,” *Eur Heart J*,37:1220–7(2016). [PubMed: 26763790]
- [24] D.Dey, S. Gaur, K. Ovrehus, et al.,” Integrated prediction of lesion-specific ischaemia from quantitative coronary CT angiography using machine learning: a multicentre study,” *Eur Radiol*,28:2655–64, (2018). [PubMed: 29352380]
- [25] R. Nakanishi, S. Sankaran, L. Grady, et al.,” Automated estimation of image quality for coronary computed tomographic angiography using machine learning,” *Eur Radiol*,1–9(2018).
- [26] R. Stebbing, A. Namburete, R. Upton, P. Leeson, J. Noble,” Data-driven shape parameterization for segmentation of the right ventricle from 3Dpt echocardiography,” *Med Image Anal*. 21:29–39(2018), [PubMed: 25577559].
- [27] A. Krizhevsky, I. Sutskever, G. Hinton, “Image-Net classification with deep convolutional neural networks,” *Advances in neural information processing systems*,1097–105, (2012)
- [28] J. Wolterink, T. Leiner, B.de Vos, W.van Hamersvelt, M. Viergever, I. Isgum,” Automatic coronary artery calcium scoring in cardiac CT angiography using paired convolutional neural networks,” *Med Image Anal.*,21:30022–6, (2016).
- [29] C. HZY, J. Park, P. Heng, S. Zhou, “Iterative multi-domain regularized deep learning for anatomical structure detection and segmentation from ultrasound images,” *Med Image Compute Assist Interv*,487–95, (2016).
- [30] H. Yang, J. Sun, H. Li, L. Wang, Z. Xu,” Deep fusion net for multi-atlas segmentation: Application to cardiac MR images,” *Med Image Comput Assist Interv*,521–8, (2016).
- [31] Tan LK, McLaughlin RA, Lim E, Abdul Aziz YF, Liew YM.,” Fully automated segmentation of the left ventricle in cine cardiac MRI using neural network regression”, *J Magn Reson Imaging*, 48:140–52, (2018). [PubMed: 29316024]
- [32] J. Betancur, F. Commandeur, M. Motlagh, T. Sharir, A. Einstein, S. Bokhari, M. Fish, et al.,” Deep learning for prediction of obstructive disease from fast myocardial perfusion SPECT: a multicenter study,” *J Am Coll Cardiol Img*, 11(11):1654-1663(2018)
- [33] A. Bhan, P. Mangipudi, A. Goyal, “Deep Learning Approach for Automatic Segmentation and Functional Assessment of LV in Cardiac MRI,” *Electronics*, 11(21):3594, (2022).
- [34] I. Goodfellow, J. Pouget, M. Mirza, B. Xu, D. Warde-Farley, S. Ozair, A. Courville, and Y. Bengio,” Generative Adversarial Nets, In *Conference on Neural Information Processing Systems*, “pages 2672–2680(2014).
- [35] A. Odena, C. Olah, and J. Shlens,” Conditional Image Synthesis with Auxiliary Classifier GANs,” In *Proceedings of the International Conference on Machine Learning*, volume 70, pages 2642–2651(2017), *JMLR. org*.
- [36] M. Mirza and S. Osindero, “Conditional generative adversarial nets,” 6 Nov 2014, <https://arxiv.org/abs/1411.1784>.
- [37] M. Wiechowski, K. Godlewski, B. Sawicki, et al.,” Monte Carlo Tree Search: a review of recent modifications and applications,” *Artif Intell Rev* 56, 2497–2562 (2023). <https://doi.org/10.1007/s10462-022-10228-y>
- [38] C. Chen, C. Qin, H. Qiu, G. Tarroni, J. Duan, W. Bai, D. Rueckert,” Deep Learning for Cardiac Image Segmentation: A Review,” *Frontiers in Cardiovascular Medicine*, Volume 7, 7: 25(2020), doi: 10.3389/fcvm.2020.00025.
- [39] A. Radford, L. Metz, and S. Chintala,” Unsupervised representation learning with deep convolutional generative adversarial networks,” conference paper at ICLR 19 November(2015), <https://arxiv.org/abs/1511.06434>.

- [40] T. Karras, S. Laine, T. Aila, “A style-based generator architecture for generative adversarial networks,” In Proceedings of the conference on Computer Vision and Pattern Recognition, 4401–4410(2019).
- [41] M. Arjovsky, S. Chintala, L. Bottou, “Wasserstein generative adversarial networks,” In Proceedings of the 34th International Conference on Machine Learning, ICML 2017, Sydney, NSW, Australia, of Proceedings of Machine Learning Research, volume 70, pages 214–223(2017). PMLR.
- [42] L. Roberts, Machine Perception of 5ree-Dimensional Solids, IEEE, New York, NY, USA, (1963).
- [43] Y. Lecun, L. Bottou, Y. Bengio, and P. Haffner, “Gradient-based learning applied to document recognition,” *Proceedings of the IEEE*, vol. 86, no. 11, pp. 2278–2324(1998).
- [44] D. Rui, G. Guo, X. Yan, B. Chen, Z. Liu, and X. He, “BiGAN: collaborative filtering with bidirectional generative adversarial networks,” in Proceedings of the 2020 SIAM International Conference on Data Mining, pp. 82–90(2020), Cincinnati, OH, USA.
- [45] J. Zhu, T. Park, P. Isola, and A. Efros, “Unpaired image-to-image translation using cycle-consistent adversarial networks,” arXiv preprint arXiv:1703.10593, (2017), <https://arxiv.org/abs/1703.10593>.
- [46] C. Ledig, L. Oeis, F. Huszar, et al., “Photo-realistic single image super-resolution using a generative adversarial network,” arXiv:1609.04802v5 [cs.CV], (2017), <https://arxiv.org/abs/1609.04802>.
- [47] A. Odena, C. Olah, and J. Shlens, “Conditional image synthesis with auxiliary classifier GANs,” (2016), <https://arxiv.org/abs/1610.09585>
- [48] E. Denton, S. Chintala, a. szlam, and R. Fergus, “Deep generative image models using a Laplacian pyramid of adversarial networks,” in Advances in Neural Information Processing Systems, vol. 28, pp. 1486–1494(2015), Curran Associates, Inc., Red Hook, NY, USA.
- [49] H. Zhang, I. Goodfellow, D. Metaxas, and A. Odena, “Self-attention generative adversarial networks,” in Proceedings of the International Conference on Machine Learning; PMLR, pp. 7354–7363(2019), Long Beach, CA, USA.
- [50] D. Im, C. Kim, H. Jiang, R. Memisevic, “Generating images with recurrent adversarial networks,” (2016), <https://arxiv.org/abs/1602.05110>.
- [51] A. Makhzani, J. Shlens, N. Jaitly, I. Goodfellow, B. Frey, “Adversarial autoencoders,” (2016), <https://arxiv.org/abs/1511.05644>.
- [52] P. Isola, J. Y. Zhu, T. Zhou, A. Efros, “Image-to-image translation with conditional adversarial networks,” in Proceedings of the IEEE Conference on Computer Vision and Pattern Recognition, pp. 1125–1134(2017), Honolulu, HI, USA.
- [53] I. Oksuz, J. Clough, W. Bai, B. Ruijsink, E. Antón, G. Cruz, C. Prieto, A. King, J. Schnabel, “High-quality segmentation of low-quality cardiac MR images using k-space artifact correction,” Proceedings of Machine Learning Research, 102:380–389(2019), <https://openreview.net/group?id=MIDL.io/2019/Conference>.
- [54] H. Zhang, X. Cao, L. Xu, L. Qi, “Conditional convolution generative adversarial network for Bi-ventricle segmentation in cardiac MR images,” ACM Int Conf Proc Ser. <https://doi.org/10.1145/3364836.3364860>.
- [55] W. Yan, Y. Wang, S. Gu, L. Huang, F. Yan, L. Xia, Q. Tao, The Domain Shift Problem of Medical Image Segmentation and Vendor-Adaptation by Unet-GAN, in book: Medical Image Computing and Computer Assisted Intervention – MICCAI 2019, (2019).
- [56] A. Chartsias, T. Joyce, G. Papanastasiou, S. Semple, M. Williams, D. Newby, R. Dharmakumar, A. Sotirios. “Tsaftaris, Factorised, spatial representation learning: application in semi-supervised myocardial segmentation,” In arXiv. Springer International Publishing, pp 490–498(2018), https://doi.org/10.1007/978-3-030-00934-2_55
- [57] M. Rezaei, H. Yang, S. Meinel, “Whole heart and great vessel segmentation with context-aware of generative adversarial networks,” Inform Aktuell, volume 11, pp 353–358(2018), https://doi.org/10.1007/978-3-662-56537-7_89
- [58] S. Dong, G. Luo, K. Wang, S. Cao, A. Mercado, O. Shmuilovich, H. Zhang, S. Li, “VoxelAtlasGAN: 3D left ventricle segmentation on echocardiography with atlas guided generation and voxel-to-voxel discrimination,” 21st International Conference, Granada, Spain, September 2018, 1806.03619 (2018), Proceedings, Part IV.
- [59] Y. Skandarani, N. Painchaud, P. Jodoin, A. Lalonde, “On the effectiveness of GAN generated cardiac MRIs for segmentation,” Medical Imaging with Deep Learning, 1–4(2020)
- [60] J. Ossenberg, V. Grau, “Conditional generative adversarial networks for the prediction of cardiac contraction from individual frames,” In Springer, pp 109–118(2019).
- [61] A. Makhzani, J. Shlens, N. Jaitly, I. Goodfellow, B. Frey, “Adversarial autoencoders,” (2016), <https://arxiv.org/abs/1511.05644>.
- [62] Z. Zhuang, P. Jin, A. Joseph, Y. Yuan, S. Zhuang, “Interactive echocardiography translation using few-shot GAN transfer learning,” Comput Math Methods Med, 2020.
- [63] C. Xu, L. Xu, P. Ohorodnyk, M. Roth, B. Chen, S. Li, “Contrast agent-free synthesis and segmentation of ischemic heart disease images using progressive sequential causal GANs,” Med Image Anal 2020, 62:101668(2020). <https://doi.org/10.1016/j.media.2020.101668>
- [64] W. Yan, Y. Wang, S. Gu, L. Huang, F. Yan, L. Xia, Q. Tao, “The domain shift problem of medical image segmentation and vendor-adaptation by Unet-GAN,” arXiv 2019, 1:623–631(2019), <https://arxiv.org/ftp/arxiv/papers/1910/1910.13681.pdf>
- [65] C. Xu, L. Xu, P. Ohorodnyk, M. Roth, B. Chen, S. Li, “Contrast agent-free synthesis and segmentation of ischemic heart disease images using progressive sequential causal GANs,” Med. Image Anal. 62:101668(2020), doi: 10.1016/j.media.2020.101668
- [66] C. Xu, L. Xu, G. Brahm, H. Zhang, S. Li, “MuTGAN: simultaneous segmentation and quantification of myocardial infarction without contrast agents via joint adversarial learning,” in Medical Image Computing and Computer Assisted Intervention – MICCAI 2018. MICCAI (2018).
- [67] K. Le, Z. Lou, W. Huo, X. Tian, “Auto Whole Heart Segmentation from CT images Using an Improved Unet-GAN,” Journal of Physics: Conference Series 1769 (2021) 012016 IOP Publishing doi:10.1088/1742-6596/1769/1/012016.
- [68] C. Decourta, L. Duongb, “Semi-supervised generative adversarial networks for the segmentation of the left ventricle in pediatric MRI,” Elsevier, Volume 123, 103884(2020), <https://doi.org/10.1016/j.compbimed.2020.103884>
- [69] Y. Zhang, L. Yang, J. Chen, M. Fredericksen, D. P. Hughes, D. Z. Chen, “Deep Adversarial Networks for Biomedical Image Segmentation Utilizing Unannotated Images,” in M. Descoteaux, Medical Image Computing and Computer Assisted Intervention MICCAI 2017, Springer International Publishing, Cham, pp. 408–416(2017).
- [70] C. Chen, W. Bai, R. Davies, A. Bhuva, C. Manisty, J. Moon, et al., “Improving the generalizability of convolutional neural network-based segmentation on CMR images,” Front. Cardiovasc. Med, 30 June 2020, Volume 7. <https://doi.org/10.3389/fcvm.2020.00105>

- [71] A. Andreopoulos, J. Tsotsos, "Efficient and generalizable statistical models of shape and appearance for analysis of cardiac MRI," *Med Image Anal.* 12:335–57(2008). doi: 10.1016/j.media.2007.12.003. Data source: <http://www.cse.yorku.ca/~mridataset/>
- [72] P. Radau, Y. Lu, G. Connelly, A. Dick, G. Wright, "Evaluation framework for algorithms segmenting short axis cardiac MRI," *MIDAS J.* 10:16:48(2009). Available online at: <http://hdl.handle.net/10380/3070>.
- [73] A. Suinesiaputra, B. Cowan, A. Al-Agamy, M. Elattar, N. Ayache, A. Fahmy, et al., "A collaborative resource to build consensus for automated left ventricular segmentation of cardiac MR images," *Med Image Anal.* 18:50–62(2014), doi: 10.1016/j.media.2013.09.001.
- [74] C. Petitjean, M. Zuluaga, W. Bai, J. Dacher, D. Grosgeorge, J. Caudron, "Right ventricle segmentation from cardiac MRI: a collation study," *Med Image Anal.* 9:187–202(2015).
- [75] R. Karim, R. Housden, M. Balasubramaniam, Z. Chen, D. Perry, A. Uddin, Y. Al-Beyatti, E. Palkhi et, "Evaluation of current algorithms for segmentation of scar tissue from late gadolinium enhancement cardiovascular magnetic resonance of the left atrium, "an open-access grand challenge." *J Cardiovasc Magn Reson.* 15:105(2015).
- [76] R. Karim, P. Bhagirath, P. Claus, R. Housden, Z. Chen, Z. Karimghaloo, H. Sohn et al, "Evaluation of state-of-the-art segmentation algorithms for left ventricle infarct from late gadolinium enhancement MR images," *Med Image Anal.* 30:95-107(2016).
- [77] C. Gomez, A. Geers, J. Peters, J. Weese, K. Pinto, R. Karim, M. Ammar, A. Daoudi, et al, "Benchmark for algorithms segmenting the left atrium from 3D CT and MRI datasets," *IEEE Trans Med Imaging.* 34(7):1460-1473(2015), doi: 10.1109/TMI.2015.2398818.
- [78] D. Pace, A. Dalca, T. Geva, A. Powell, M. Moghari, P. Golland, "Interactive whole-heart segmentation in congenital heart disease," *Med Image Comput Comput Assist Interv.* 9351:80–8(2015). doi: 10.1007/978-3-319-24574-4_10.
- [79] O. Bernard, A. Lalonde, C. Zotti, F. Cervenansky, X. Yang, P. Heng, I. Cetin, K. Lekadir, O. Camara et al, "Deep learning techniques for automatic MRI cardiac multi-structures segmentation and diagnosis: is the problem solved?" *IEEE Trans Med Imaging.* 37:2514–25(2018). doi: 10.1109/TMI.2018.2837502
- [80] J. Zhao, Z. Xiong, Left Atrial Segmentation Challenge Dataset (2018). available online at: <http://atriaseg2018.cardiacatlas.org/>.
- [81] X. Zhuang, L. Li, C. Payer, D. Stern, M. Urschler, M. Heinrich, et al., "Evaluation of algorithms for multi-modality whole heart segmentation: an open-access grand challenge," *Med Image Anal.* 58:101537(2019). doi: 10.1016/j.media.2019.101537.
- [82] M. Schaap, T. Coert, T. Walsum, A. Giessen, A. Weustink, et al., "Standardized evaluation methodology and reference database for evaluating coronary artery centerline extraction algorithms," *Med Image Anal.* 13:701–14(2009). doi: 10.1016/j.media.2009.06.003.
- [83] H. Kirişli, M. Schaap, C. Metz, A. Dharampal, W. Meijboom, S. Papadopoulou, A. Dedic, K. Nieman, M. Graaf, M. Meijs, M. Cramer et al., "Standardized evaluation framework for evaluating coronary artery stenosis detection, stenosis quantification, and lumen segmentation algorithms in computed tomography angiography," *Med Image Anal.* 17:859–76(2013). doi: 10.1016/j.media.2013.05.007.
- [84] O. Bernard, J. Bosch, B. Heyde, M. Alessandrini, D. Barbosa, S. Camarasu, F. Cervenansky et al., "Standardized evaluation system for left ventricular segmentation algorithms in 3D echocardiography," *IEEE Trans Med Imaging.* 35:967–77(2016). doi: 10.1109/TMI.2015.2503890
- [85] S. Leclerc, E. Smistad, J. Pedrosa, A. Ostvik, F. Cervenansky, F. Espinosa, T. Espeland, et al., "Deep learning for segmentation using an open large-scale dataset in 2D echocardiography", *IEEE Trans Med Imaging.* 38:2198–210(2019). doi: 10.1109/TMI.2019.2900516.